

THEORETICAL NEUROSCIENCE I

Lecture 2: Single compartment model

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Content

1. Equivalent circuits
2. Hydraulic analogue
3. Single-compartment model
4. Solving for voltage
5. Solving for currents
6. Ion-specific conductances

1 Equivalent circuits

The biophysical components of a neuron (i.e., cell membranes, intracellular plasma, channel proteins, etc) behave like electronic circuit components and are characterized by electrical *voltage*, *current*, *resistance*, *conductance*, *capacitance*, and so on.

We take advantage of this fact and describe neurons in terms of electronic *equivalent circuits*.

Axon lumen (Ohm's Law with resistance)

As a first example, consider an axon segment of length L and radius a . This segment presents an electrical resistance R_L to longitudinal currents:

$$R_L = \frac{r_L L}{\pi a^2} \quad r_L \text{ resistivity}$$

for example $L = 100 \mu m$ $a = 2 \mu m$ $r_L \approx 1 \text{ k}\Omega \text{ mm}$

$$R_L = \frac{1 \text{ k}\Omega \text{ mm} \cdot 0.1 \text{ mm}}{\pi \cdot 0.002^2 \text{ mm}^2} \approx 8 \text{ M}\Omega$$

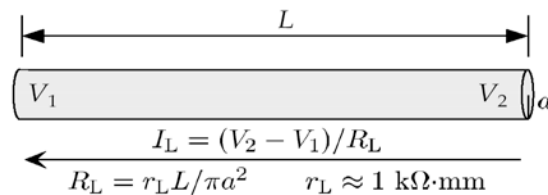


Figure 1: Ohm's law resistance. [1]

Ohm's Law:

Resistance is the ratio between voltage drop and current or, equivalently, voltage drop is the product of resistance and current:

$$R[\text{Ohm}] = \frac{V[\text{Volt}]}{I[\text{Ampere}]} \quad \Leftrightarrow \quad V[\text{Volt}] = R[\text{Ohm}] I[\text{Ampere}]$$

Causation works both ways! Voltage drops cause currents to flow.

Flowing currents cause voltage drops.

For example, the voltage drop V_L required to drive a current $I_L = 1 \text{ nA}$ through this axon segment:

$$V_L = 8 \text{ M}\Omega \cdot 1 \text{ nA} = 8 \times 10^{+6} \Omega \cdot 1 \times 10^{-9} \text{ A} = 8 \times 10^{-3} \text{ V} = 8 \text{ mV}$$

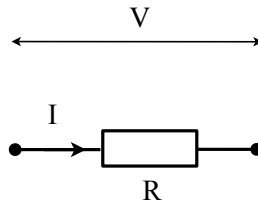


Figure 2: Circuit diagram with resistance R , voltage drop V , and current I .

Channel pore (Ohm's Law with conductance)

Consider a channel protein with a cylindrical pore of $L_C = 6 \text{ nm}$ length and crosssectional area of $A_C = 0.15 \text{ nm}^2$ and its *conductance* G_C (inverse of resistance):

$$G_C = \frac{1}{R_C} = \frac{A_C}{r_L L_C} \approx \frac{0.15 \text{ nm}^2}{1 \text{ k}\Omega \text{ mm} \cdot 6 \text{ nm}} \approx \frac{1}{40 \text{ G}\Omega} = 25 \text{ pS}$$

For conductance, **Ohm's Law** takes a slightly different form:

$$V[\text{Volt}] = \frac{I[\text{Ampere}]}{G[\text{Siemens}]} \quad \Leftrightarrow \quad I = GV \quad S \equiv \frac{A}{V} = \Omega^{-1}$$

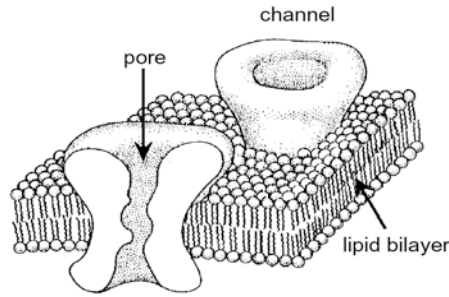


Figure 3: Channel pore [2]

Ion-specific conductance

Membranes with ion-specific channel proteins exhibit an ion-specific conductance. For the ion in question, the driving force is the difference between membrane potential and reversal potential. We modify Ohm's Law as follows:

$$I_X = G_X (V - E_X)$$

The conductance G_X needs to be calculated from the *resistivity* r_X (or *conductivity* g_X) and the cells surface area a :

$$G_X = g_X a = \frac{a}{r_X} = \frac{0.01 \text{ mm}^2}{1 \text{ M}\Omega \text{ mm}^2} = 10 \text{ nS}$$

where we have used typical values for r_X and a .

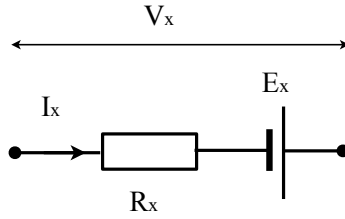


Figure 4: The ‘equivalent circuit’ of an ion-specific conductance is a resistance R_x (conductance) in series with a battery (reversal potential E_x).

Membrane capacitance

The membrane capacitance is governed by the *capacitor equation*:

$$Q[\text{Coulomb}] = C_m[\text{Farad}] V_m[\text{Volt}]$$

$$C_m[F] = c_m[F \text{ mm}^{-2}] A[\text{mm}^2], \quad c_m \approx 10 \text{ nF/mm}^2$$

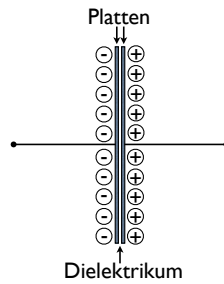


Figure 5: Membrane capacitance.

Time-derivative of capacitor equation

The charge Q changes only when a current I_m flows through the membrane:

$$\frac{dQ}{dt} = I_m \quad 1A = \frac{1\text{Coulomb}}{1s}$$

Thus, the time derivative of the capacitor equation relates current *through* and voltage *across* a membrane:

$$I_m = \frac{dQ}{dt} = C_m \frac{dV_m}{dt}$$

Circuit diagram

In a capacitance, current and voltage are not proportional. Instead, current is proportional to the voltage change!

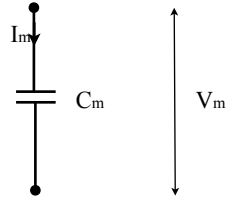


Figure 6: 'Equivalent circuit' of membrane capacitance C_m , with voltage V_m and current I_m .

2 Hydraulic analogues

Electrical quantity	Symbol	Physical unit	Hydraulic analogue
Voltage difference	V, U, v	Volt V, mV	pressure difference
Current flow	I, i	Ampère $A, mA, \mu A$	liquid flow
Resistance	R, r	Ohm $\Omega, k\Omega, M\Omega$	constriction
Conductance	G, g	Siemens $S, \mu S, pS$	opening

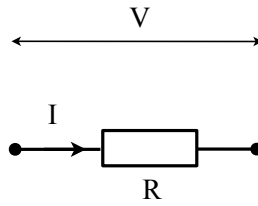


Figure 7: Circuit diagram with resistance R , voltage drop V , and current I .

Battery, voltage source

Electrical quantity	Symbol	Physical unit	Hydraulic analogue
Voltage difference	V, U, v	Volt V, mV	pressure pump
Current flow	I, i	Ampère $A, mA, \mu A$	liquid flow

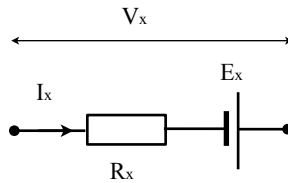


Figure 8: Circuit diagram with resistance R , voltage drop V , current I and battery E .

Capacitance

Electrical quantity	Symbol	Physical unit	Hydraulic analogue
Voltage change	$\frac{dV}{dt}, \frac{dv}{dt}$	$\frac{V}{s}$ or $\frac{mV}{ms}$	pressure change
Current flow	I, i	$A, mA, \mu A$	liquid flow
Capacitance	C, c	Farad $F, \mu F, nF$	elastic balloon

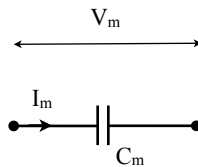


Figure 9: Circuit diagram v, i and c .

Hydraulic analogue of ‘single-compartment model’

Voltage = pressure, current = flow

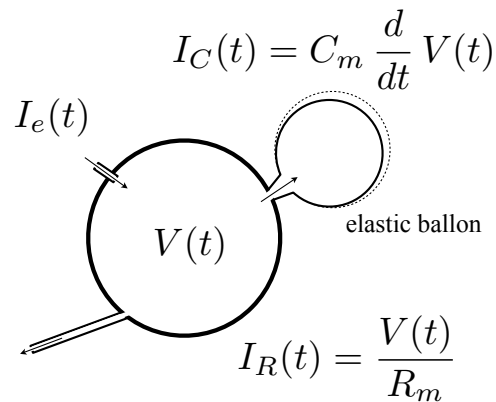


Figure 10: Single-compartment model. [3]

3 Single-compartment model

At the soma of a neuron, the membrane potential is relatively uniform across the entire surface. The soma is **“electrotonically compact”** and can be treated as a single **“compartment”**. Such a compartment is characterized by a single membrane potential, membrane capacity, and membrane resistance. Typical values are:

$$R_m \approx \frac{1 \text{ M}\Omega\text{mm}^2}{0.1 \text{ to } 0.01 \text{ mm}^2} = 10 \text{ to } 100 \text{ M}\Omega$$

$$C_m \approx 10 \text{ nF/mm}^2 \cdot (0.1 \text{ to } 0.01 \text{ mm}^2) = 0.1 \text{ to } 1 \text{ nF}$$

$$\tau_m = R_m C_m \approx 10 \text{ ms to } 100 \text{ ms.}$$

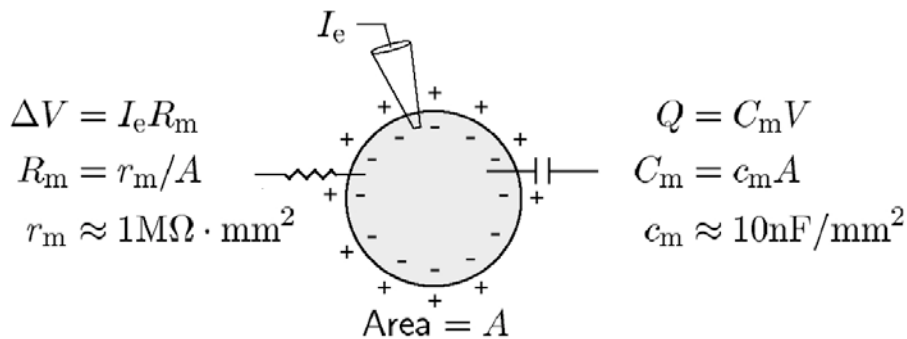


Figure 11: Single membrane potential. [4]

Basic equation

We now derive the basic equation of the single-compartment model. In addition to membrane resistance and capacitance, we consider an electrode, which has been inserted in the soma and which can serve two functions: it can deliver current and it can measure voltage. As always,

we define the membrane current as an *outward* current. For an electrode current, the convention is different: it is defined as an *inward* current. Due to this convention, the inward electrode current (which may be zero) must equal the outward membrane currents:

$$I_e = I_R + I_C$$

Using Ohm's Law and the Capacitor Equation, we can express both components of the membrane current in terms of the membrane potential:

$$I_e = \frac{V_m}{R_m} + C_m \frac{dV_m}{dt}$$

$$I_R = \frac{V_m}{R_m} \qquad I_C = C_m \frac{dV_m}{dt}$$

This is the **basic equation** of the single-compartment model.

Alternative form

Often, this equation is written not in absolute but in 'specific' quantities (per unit membrane area). In this case, the equation reads

$$\frac{I_e}{A} = \frac{V_m}{r_m} + c_m \frac{dV_m}{dt}$$

Recall that we use capital letters (R_m , C_m) for absolute resistance and capacitance, but lower case letters (r_m , c_m) for resistivity and conductivity.

Equivalent circuit

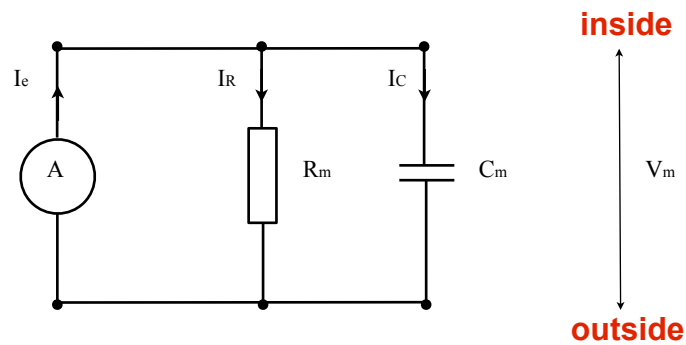


Figure 12: Parallel circuit diagram.

$$I_e = \frac{V_m}{R_m} + C_m \frac{dV_m}{dt}$$

Hydraulic analogue

Voltage = pressure, current = flow

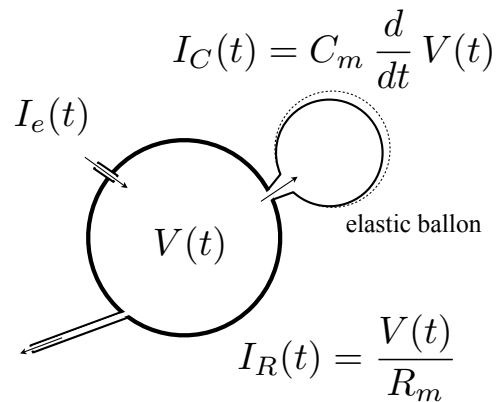


Figure 13: Single-compartment model. [3]

4 Solving for voltage

Given an arbitrary input current $I_e(t)$, we'd like to know:

- Membrane voltage $V_m(t)$ over time.
- Resistive current $I_R(t)$ over time.
- Capacitative current $I_C(t)$ over time.

Initially, we restrict ourselves to a constant input current $I_e(t) = I_0$. Later on, we shall generalize to time-varying inputs.

Time constant and equilibrium potential

To begin to understand the implications of our basic equation, we introduce the **membrane time-constant**

$$\tau_m = R_m C_m$$

and rearrange to isolate the voltage change:

$$\tau_m \frac{dV(t)}{dt} = -V(t) + R_m I_0$$

While I_0 remains constant, the potential will move towards a particular value, namely, $R_m I_0$. (As long as V is less than this value, dV is positive and V will increase. As long as V is larger than this value, dV is negative and V will decrease.)

Accordingly, we can consider $R_m I_e$ as an **equilibrium potential** V_∞ (dt. Grenzpotential).

$$0 = \tau_m \frac{dV(t)}{dt} = -V(t) + R_m I_e \quad \Rightarrow \quad V_\infty = R_m I_0$$

Our equation now reads

$$\tau_m \frac{dV(t)}{dt} = -V(t) + V_\infty$$

or

$$\frac{dV(t)}{dt} = -\frac{1}{\tau_m} [V(t) - V_\infty]$$

Exponential relaxation

The basic equation of our single-compartment model is a common linear differential equation (LDE), which describes an **exponential relaxation**. We speak of an exponential relaxation when a state variable x always returns ('relaxes') towards some equilibrium value and when the speed of this movement is proportional to the distance from the equilibrium value.

$$\frac{dV(t)}{dt} = -\frac{1}{\tau} [V(t) - V_\infty]$$

where V_∞ is the equilibrium value, and τ is the relaxation time.

Solution With $V(0) = V_0$, the solution is

$$V(t) = V_\infty + (V_0 - V_\infty) \exp\left(-\frac{t}{\tau}\right)$$

To check, differentiate the solution to obtain the left-hand side of the LDE:

$$LHS = \frac{dV(t)}{dt} = -\frac{1}{\tau} (V_0 - V_\infty) \exp\left(-\frac{t}{\tau}\right)$$

and substitute the solution $V(t)$ to obtain the right-hand side:

$$RHS = -\frac{1}{\tau} [V(t) - V_\infty] = -\frac{1}{\tau} (V_0 - V_\infty) \exp\left(-\frac{t}{\tau}\right)$$

$$\frac{dV(t)}{dt} = -\frac{1}{\tau} [V(t) - V_{\infty}] \quad V(0) = V_0$$

$$V(t) = V_{\infty} + (V_0 - V_{\infty}) \exp\left(-\frac{t}{\tau}\right)$$

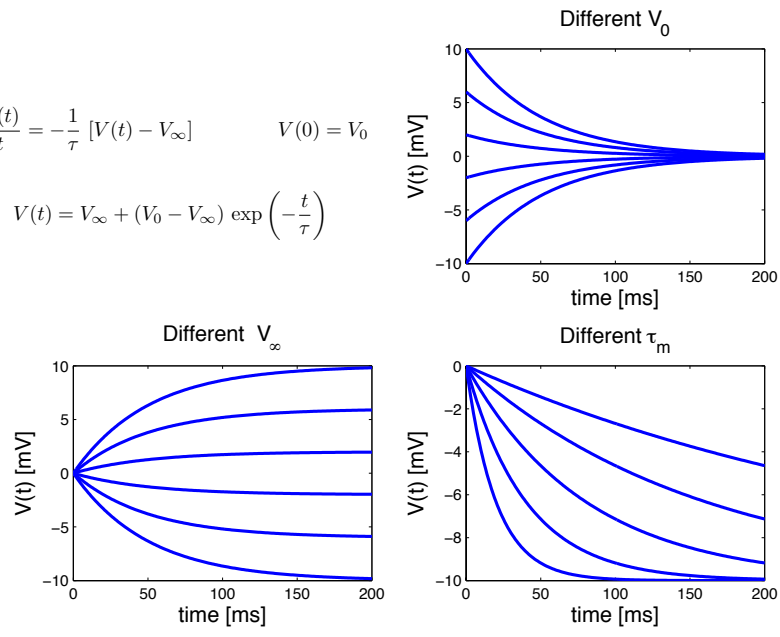


Figure 14: Find that both sides are identical. QED.

5 Solving for currents

Exact solution for a step-like input current:

$$\tau_m \frac{dV(t)}{dt} = -V(t) + V_\infty(t), \quad V(0) = 0$$

$$\tau_m = R_m C_m \quad V_\infty(t) = R_m I_e(t) = \begin{cases} R_m I_0 & t \geq 0 \\ 0 & t < 0 \end{cases}$$

The solution for the membrane potential is

$$V(t) = V_\infty - V_\infty \exp\left(-\frac{t}{\tau_m}\right)$$

Membrane currents

Given this solution, we can use Ohm's law and the capacitor equation

$$I_R = \frac{V(t)}{R_m} \quad I_C = C_m \frac{dV(t)}{dt}$$

to compute the resistance current

$$I_R = \frac{V_\infty}{R_m} \left[1 - \exp\left(-\frac{t}{\tau_m}\right)\right] = I_0 \left[1 - \exp\left(-\frac{t}{\tau_m}\right)\right]$$

and the capacitance current

$$I_C = C_m \frac{-1}{\tau_m} \left[-V_\infty \exp\left(-\frac{t}{\tau_m}\right)\right] = I_0 \exp\left(-\frac{t}{\tau_m}\right)$$

Current division

Now we know how the additional current is divided between resistance and capacitance, and how this division changes over time:

$$V(t) = V_{\infty} \left[1 - \exp\left(-\frac{t}{\tau_m}\right) \right] \quad I_R = I_e \left[1 - \exp\left(-\frac{t}{\tau_m}\right) \right] \quad I_C = I_e \exp\left(-\frac{t}{\tau_m}\right)$$

```
function SCM
    tau = 20;
    t = 0:1:100;
    Vinf = 100;
    Ie = 10;
    V = Vinf * (1 - exp(-t/tau));
    IR = Ie * (1 - exp(-t/tau));
    IC = Ie * exp(-t/tau);

    figure;
    subplot(1,3,1);
    plot(t,V,'LineWidth',2.0);
    xlabel('time t', 'FontSize', 24);
    ylabel('voltage V', 'FontSize', 24);
    axis 'square';

    subplot(1,3,2);
    plot(t,IR,'LineWidth',2.0);
    xlabel('time t', 'FontSize', 24);
    ylabel('current I_R', 'FontSize', 24);
    axis 'square';

    subplot(1,3,3);
    plot(t,IC,'LineWidth',2.0);
    xlabel('time t', 'FontSize', 24);
    ylabel('current I_C', 'FontSize', 24);
    axis 'square';

    return;
```

Figure 15: Matlab script for plots

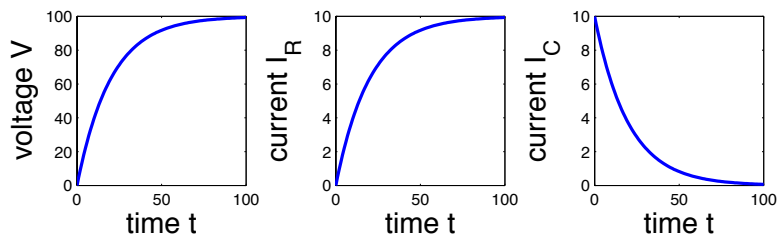


Figure 16: Plots time vs. voltage V , current I_R and current I_C

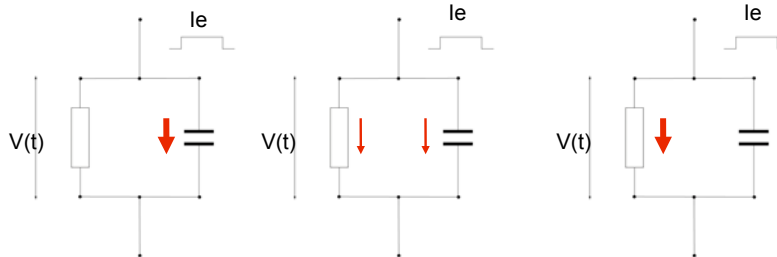


Figure 17: Equivalent electric diagrams for plots.

Hydraulic analogue, again

Voltage = pressure, current = flow

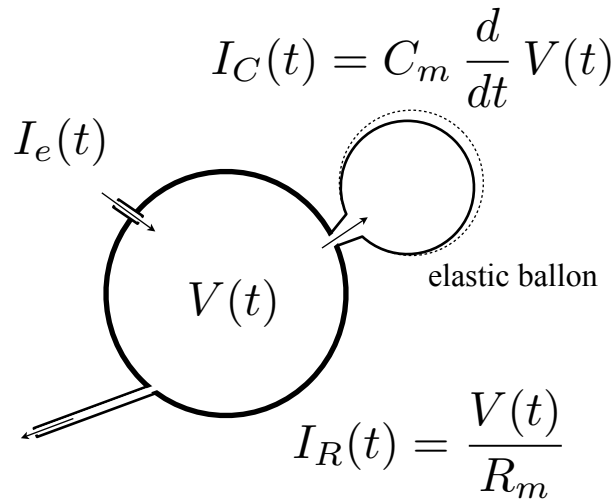


Figure 18: Single-compartment model. [3]

Some implications

With a time-varying electrode current $I_e(t)$ and equilibrium potential $V_\infty(t)$, we have

$$\tau_m \frac{dV(t)}{dt} = -V(t) + V_\infty(t),$$

$$\tau_m = R_m C_m, \quad V_\infty(t) = R_m I_e(t)$$

$$I_R = V_m(t)/R_m, \quad I_C = C_m \frac{dV_m(t)}{dt}$$

- Which quantities change *instantaneously* with a step change in the input current?
- Which quantities change *gradually* over time?
- How does the membrane potential behave?
- Where does the input current flow? Initially? After the membrane potential has equilibrated?
- How quickly does the membrane potential equilibrate?
- What are the effects of a step change in the membrane resistance?

6 Ion-specific currents (advanced)

So far, we have ignored the fact that membrane currents are carried by particular ions. We now make our single-compartment model more realistic by taking into account ion-specific conductances and reversal potentials. In our basic equation, we make explicit the membrane current *per unit area*, i_m :

$$c_m \frac{dV_m}{dt} = -i_m + \frac{I_e}{A}$$

In the past, we have calculated i_m from the membrane potential V_m and the total membrane resistance r_m .

$$i_m = \frac{V_m}{r_m}$$

Now we want to substitute a more detailed expression, which takes ion-specific conductances into account.

Single ion conductance

Total membrane current carried by ion X , with reversal potential E_X and conductivity g_X ($= \frac{1}{r_X}$).

$$c_m \frac{dV_m}{dt} = -i_m + \frac{I_e}{A} \qquad i_m = g_X(V_m - E_X)$$

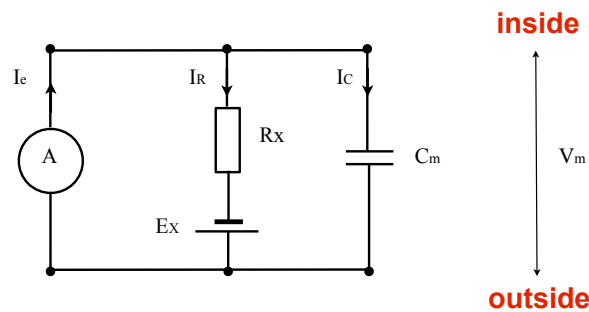


Figure 19: Electric diagram.

Multiple ion conductances

Total membrane current carried by several ions, say Na^+ and K^+ , we need to take into account the reversal potential and specific conductivity of each ion:

$$c_m \frac{dV_m}{dt} = -i_m + \frac{I_e}{A} \quad i_m = g_{Na} (V_m - E_{Na}) + g_K (V_m - E_K)$$

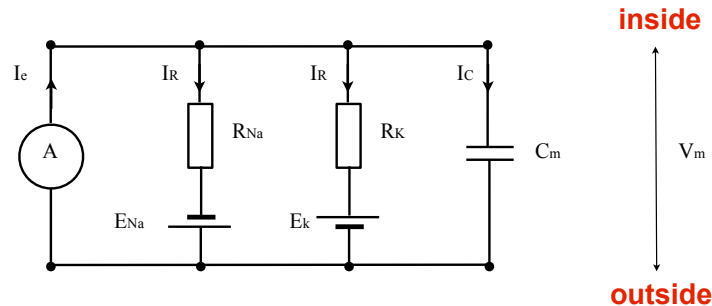


Figure 20: Electric diagram including Na and K as batteries.

Synaptic conductances

Total membrane current includes synaptic currents, also carried by particular ions. In contrast to ‘normal’ ionic conductances, synaptic conductances vary over time (depending on pre-synaptic activity):

$$i_m = g_{syn}(t) (V_m - E_{syn}) + g_{Na} (V_m - E_{Na}) + g_K (V_m - E_K)$$

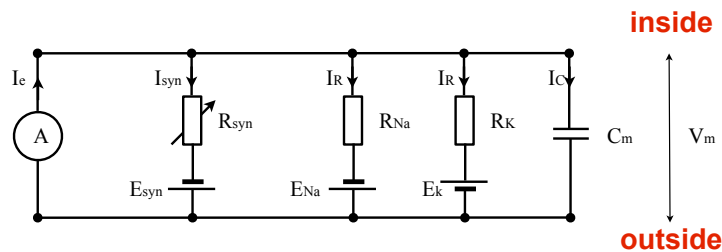


Figure 21: Electric diagram including the synaptic activity.

Generalization

The membrane current is the sum of all currents through the different types of ion channels, indexed by i . This includes leakage channels, voltage-gated channels, and synaptic channels (which are ligand-gated).

For ion-selective channels, the current vanishes when the membrane potential V equals the reversal potential E_i . For other values of V , the current increases or decreases linearly with $V - E_i$. Accordingly, $V - E_i$ can be considered the **driving force** for currents through conductance i .

We can now compute the membrane current per unit area i_m from the conductances g_i per unit area and the reversal potentials E_i :

$$c_m \frac{dV_m}{dt} = -i_m + \frac{I_e}{A} \qquad i_m = \sum_i g_i (V - E_i)$$

For example, a particular neuron might have channels for K^+ , Na^+ , Ca^{2+} , and Cl^- . In this case, we might write:

$$i_m = g_{K^+} (V - E_{K^+}) + g_{Na^+} (V - E_{Na^+}) + g_{Ca^{2+}} (V - E_{Ca^{2+}}) + \\ + g_{Cl^-} (V - E_{Cl^-}) + g_L (V - E_L)$$

where g_L and E_L are the effective conductance and reversal potential of all remaining channels (including ion pumps), that are not explicitly included.

Channels with $E_i \approx V_{rest}$ are sometimes called **shunt** conductances (e.g., Cl^-).

Summary of 'Ion-specific conductances'

- Ion-specific conductances take reversal potential into account
- Total conductance is sum of individual conductances
- Total current is sum of individual currents
- Synaptic conductances are treated in the same way

7 Bibliography

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